

# Applied Radiation Physic Group

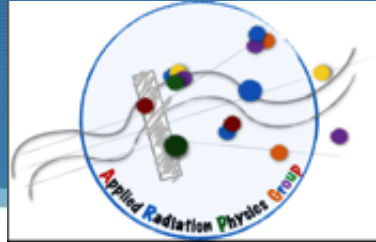
Available Thesis





SAPIENZA  
UNIVERSITÀ DI ROMA

# ARPG



## NUCLEAR MEDICINE

CHIRONE  
(Radio Guided Surgery)

WIDMAPP  
(Dosimetry for Target Radio  
Therapy)

DOSE PROFILER  
(Particle Therapy dosimetry)

## HADRON THERAPY

FOOT  
(RBE in PT)

FRED  
(TPS with GPU)

MONDO  
(Fast Neutron Detection)

PAPRICA

GENIALE  
(Low Energy Nuclear Interactions)

## ARTIFICIAL INTELLIGENCE IN MEDICINE

MARIANNE  
(Imaging for stadiation)

NEPTUNE  
(<sup>19</sup>F-MRI)

FILOBLU  
(Patient-Doctor  
interactions)

# Collaborations

Activity driven by medical input, with involvement of SMEs



NUCLEONE



Gemelli



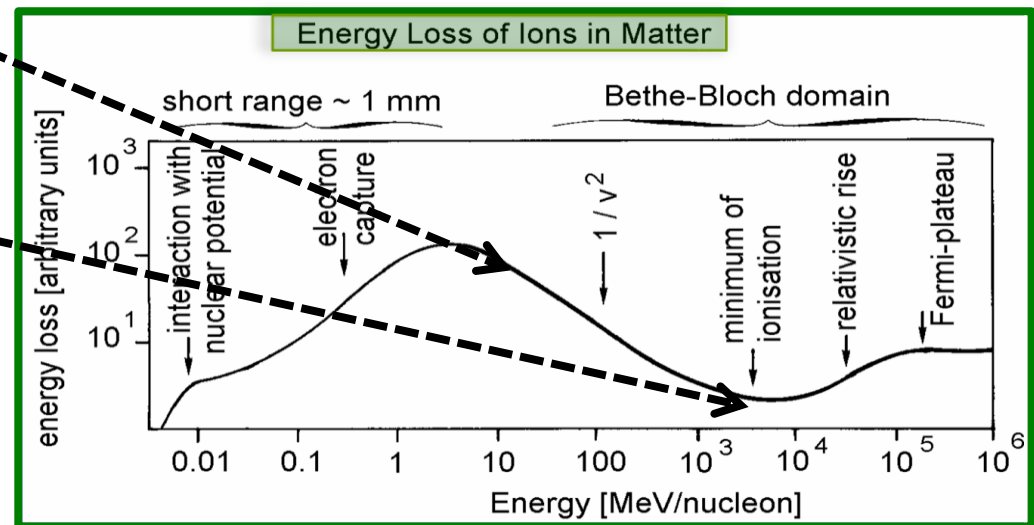
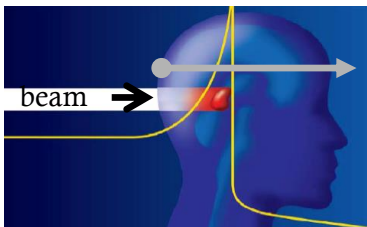
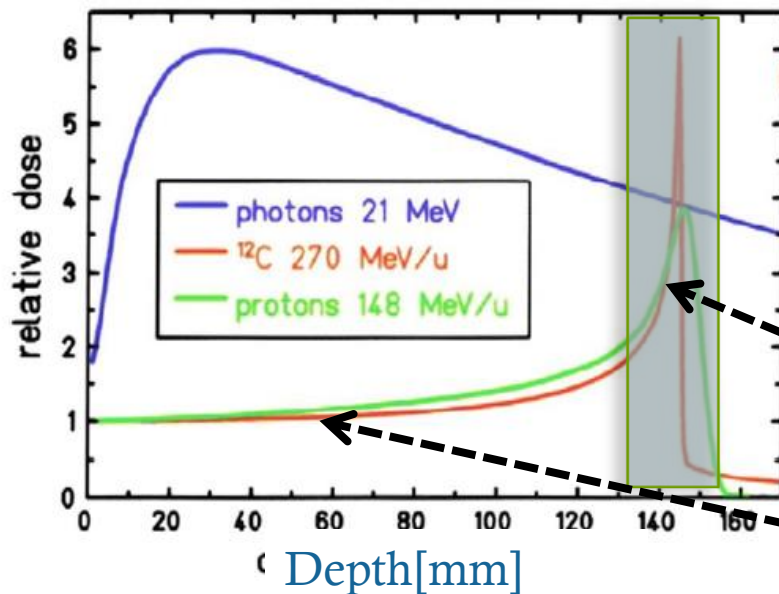
# HADROTHERAPY



# Hadrotherapy

Proton/ion beams on patient

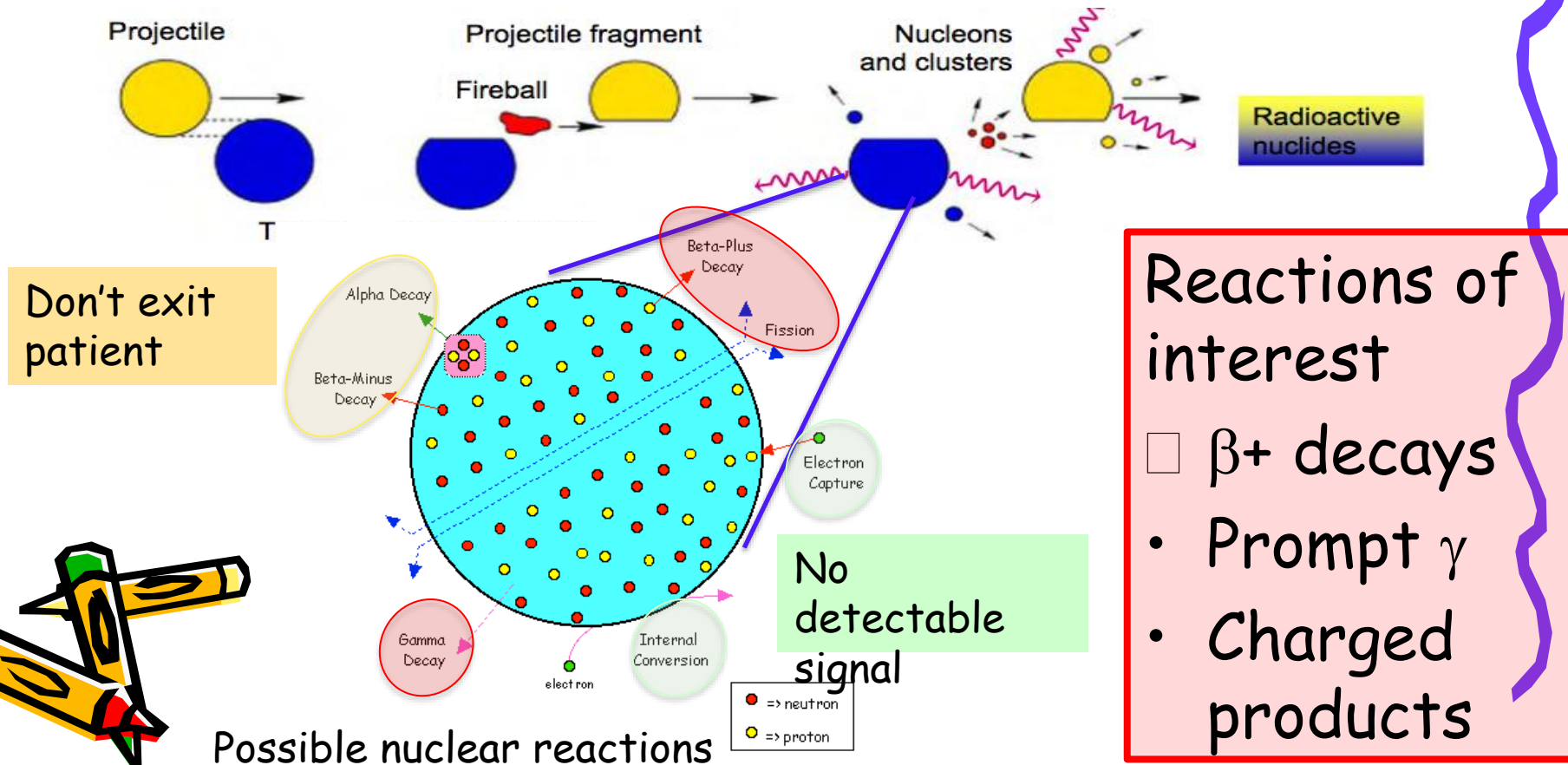
Concentrate release of energy inside **tumor** due to release of energy in ionization.



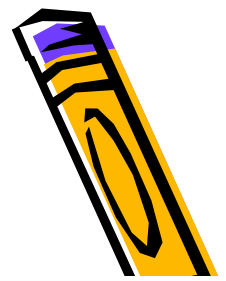
# Measuring the dose

RF, V. Patera,  
"Dose Monitoring in  
Particle Therapy",  
Mod. Phys. Lett. A

Based on nuclear reactions between  
the projectile and the patient



# Correlation between activity and dose

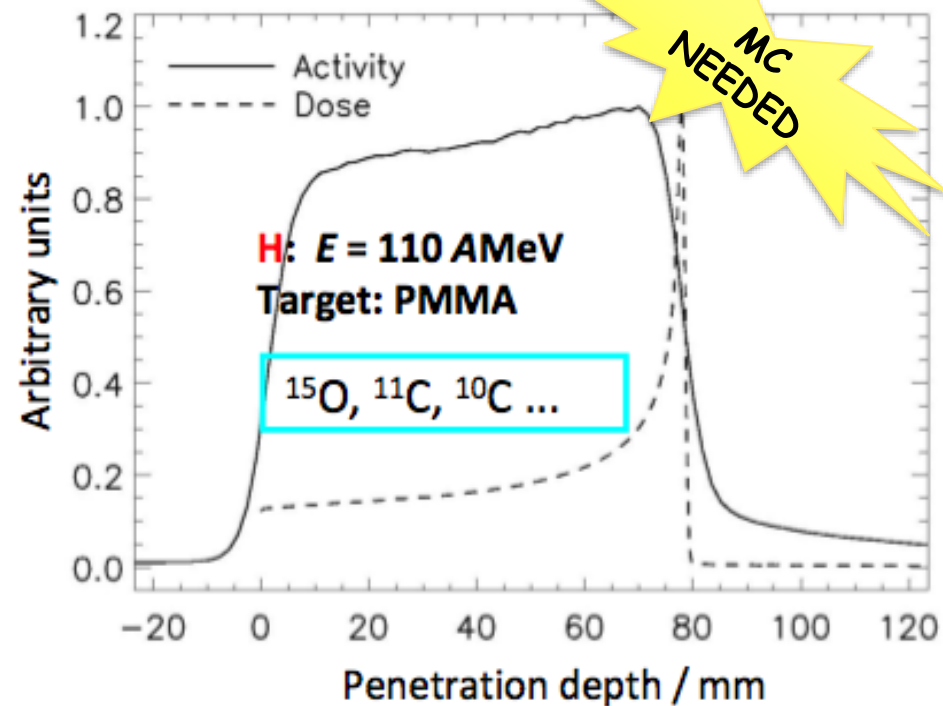
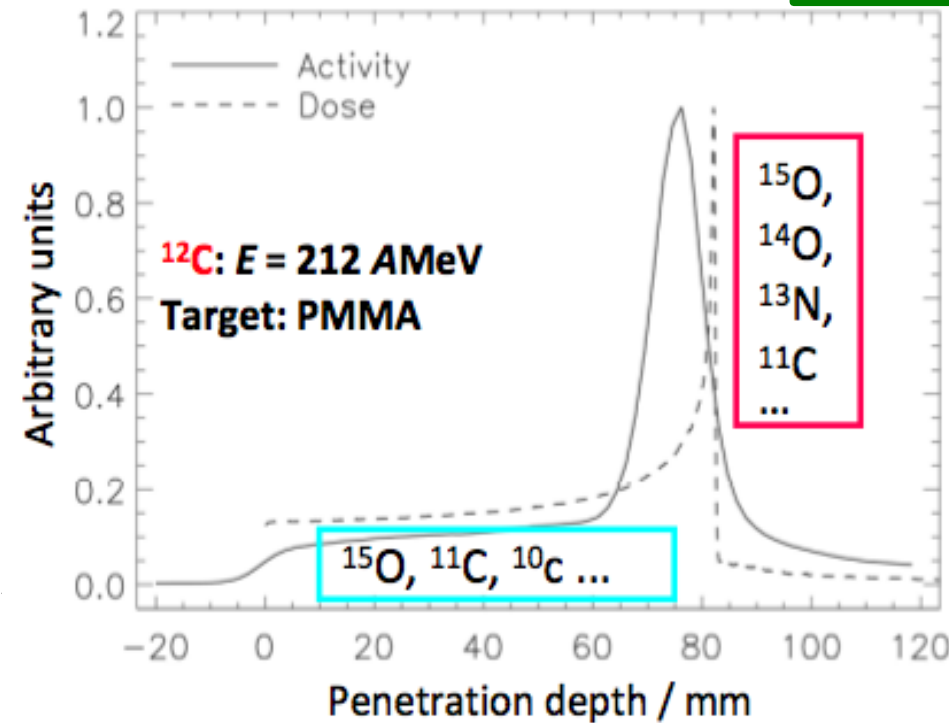


Therapy beam	$^1\text{H}$	$^3\text{He}$	$^7\text{Li}$	$^{12}\text{C}$	$^{16}\text{O}$	Nuclear medicine
Activity density / $\text{Bq cm}^{-3} \text{ Gy}^{-1}$	6600	5300	3060	1600	1030	$10^4 - 10^5 \text{ Bq cm}^{-3}$

Projectiles & target fragmentation

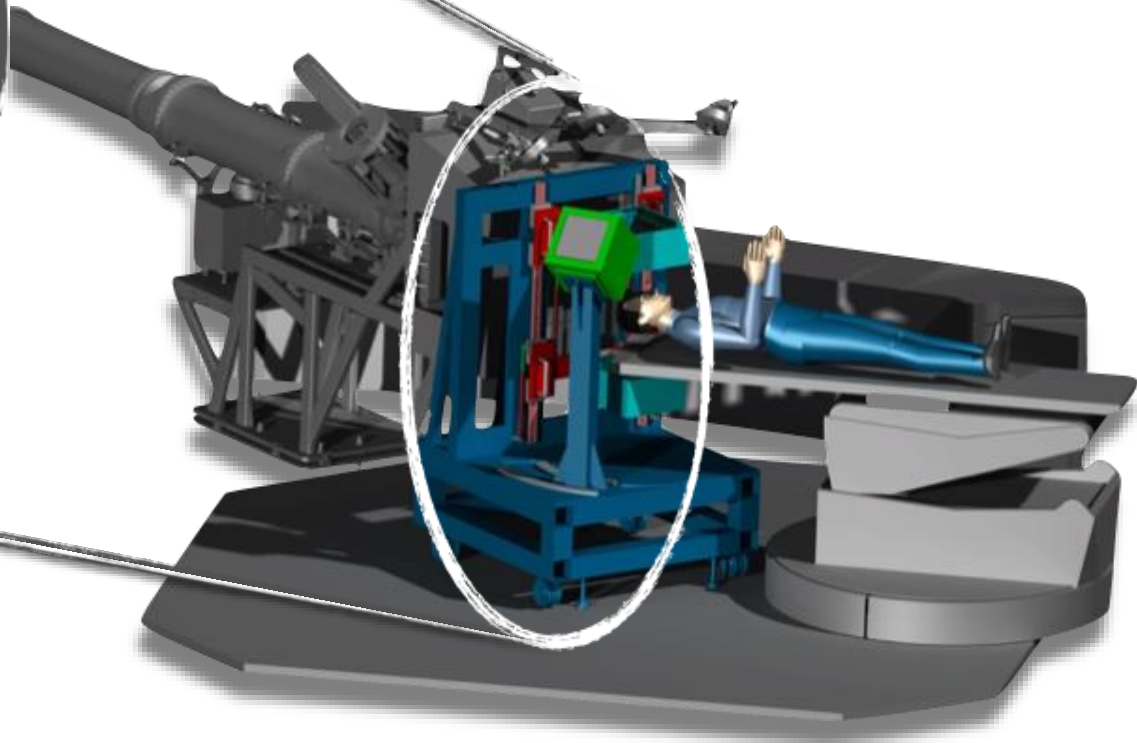
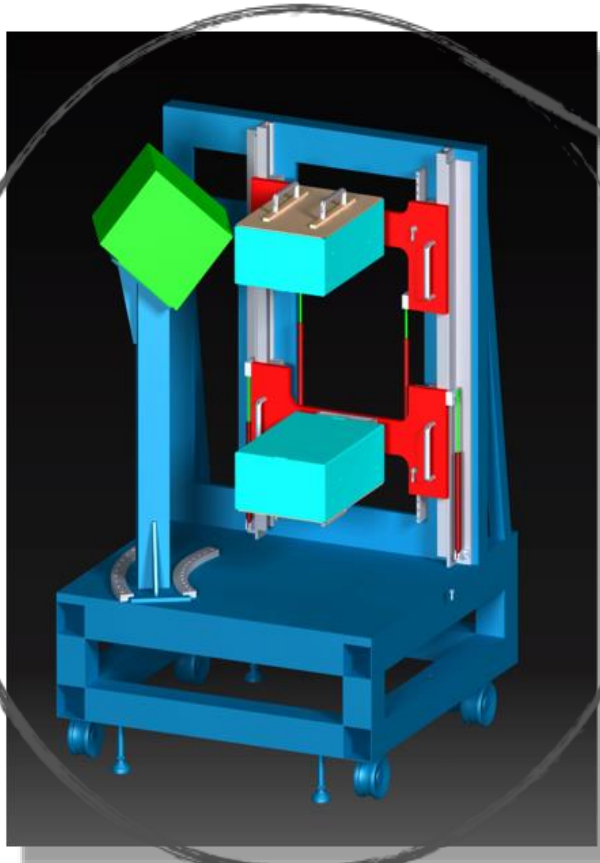
Target fragmentation

Example of  $\beta^+$



## Range monitor applications

- ◆ To exploit the secondary particles detections as an online monitor, a **Dose Profiler** has been designed (within the INSIDE Italian project) to be deployed in the CNAO treatment center.



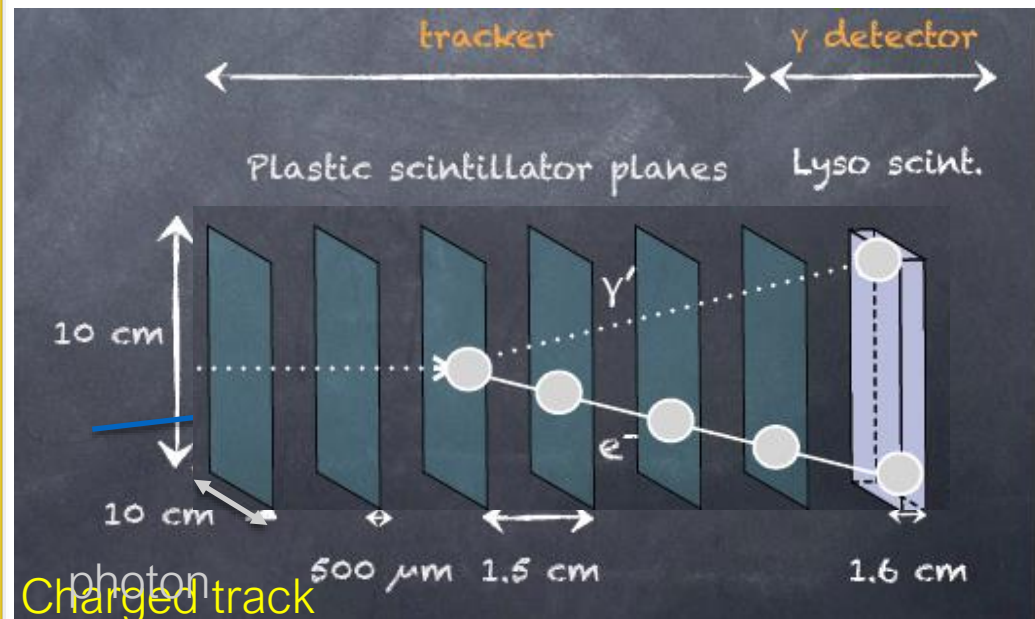
Project funded as a part of  
**INSIDE Prin**, **INFN RDH**  
and **Premiale C.F.**



# Dose Profiler

Need a detector to simultaneously measure the rate of:

- charged particles with multilayer for track reconstruction
- single photons with compton camera



# THE PAPERICA REVOLUTION

## NOVEL 3D PGI STRATEGY: PROOF OF PRINCIPLE

### Exploiting Pair Production (PP)

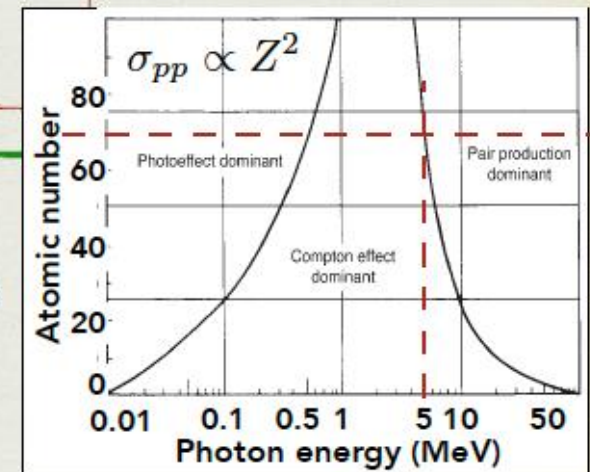
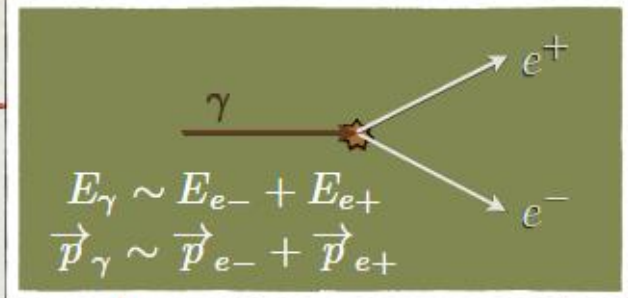
Technique used by **pair telescopes** in astrophysics applications for cosmic photons imaging  $E > 30$  MeV

**Never explored in the lower PG energy range**

$E \sim 1-10$  MeV (low cross section  $\sigma_{pp}$ )

$\Rightarrow$  Intrinsic threshold of  $\sim 4$  MeV

- **Targeted PG**  $E > 4$  MeV **more correlated with BP**
- **Reduction** of background from **uncorrelated photons** induced by neutrons (low E)
- topological event signature: **neutrons discrimination**
- No need of collimation
- **No TOF information needed**
- Allow to **3D reconstruct** the PG emission point



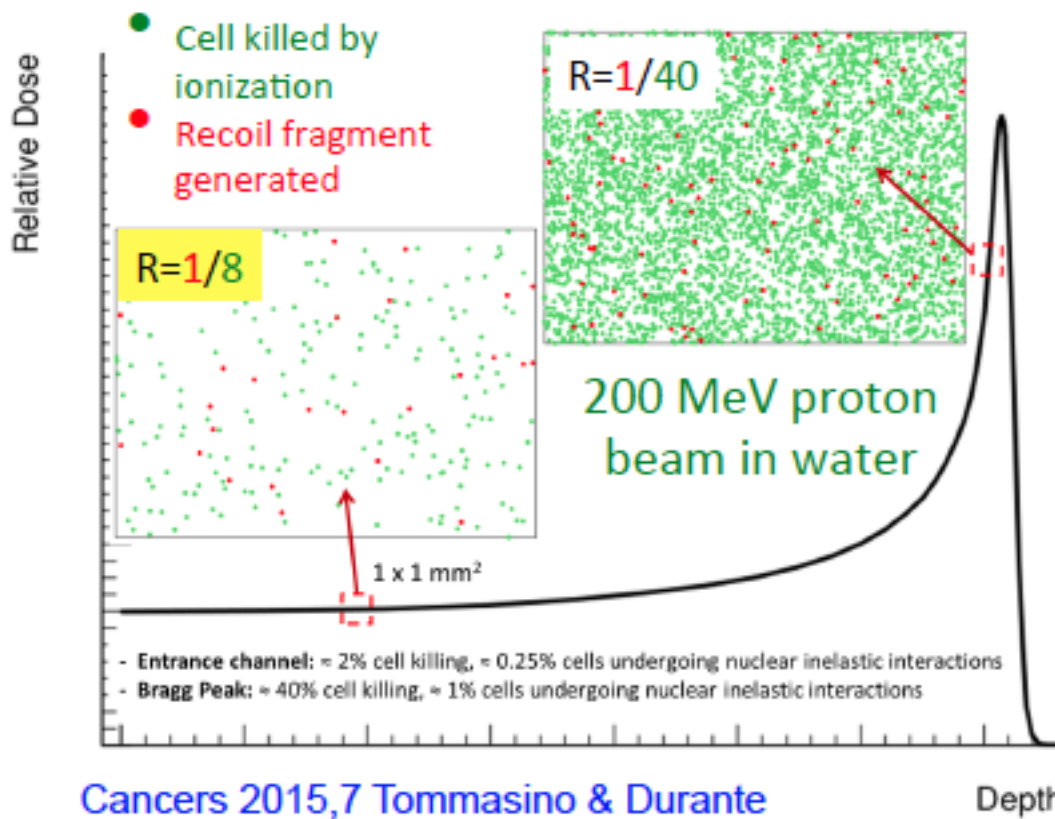
ALSO for  
 $^{12}\text{C}$  Beam

PAPERICA



# Target (patient) fragmentation & PT

Target fragmentation in proton therapy: gives contribution also outside the tumor region!



About 10% of biological effect in the entrance channel due to secondary fragments (Grun 2013)

Largest contributions of recoil fragments expected from **He, C, Be, O, N**  
In particular on Normal Tissue Complication Probability

See also :

- Paganetti 2002 PMB
- Grassberger 2011 PMB



## p-> C, p->O scattering @200 MeV

The elastic interaction and the forward Z=1 fragment production (p,d,t) are quite well known. Large uncertainty on large angle Z=1,2 fragments.

Missing data on heavy fragments. Unreliable nuclear models

“Heavy” (A>4)  
fragment yields  
and emission  
energy ~ unknown

Very low energy-  
short range  
fragments.

MCs confirm this  
picture

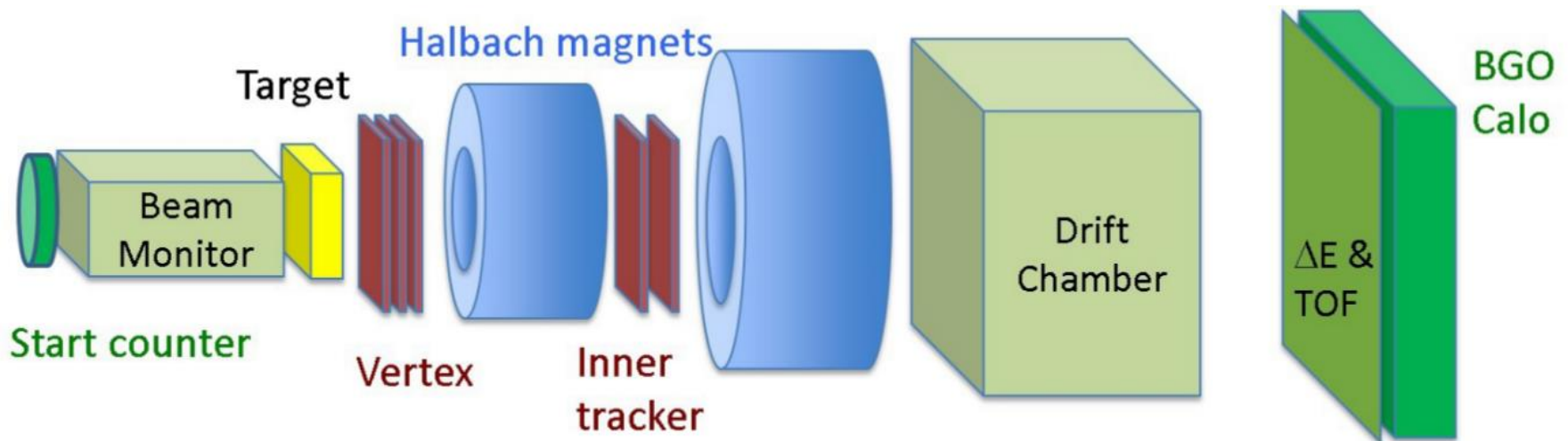
Nuclear model &  
MC not reliable

Analytic model results on p->O @200 MeV

Fragment	E (MeV)	LET (keV/ $\mu$ m)	Range ( $\mu$ m)
<sup>15</sup> O	1.0	983	2.3
<sup>15</sup> N	1.0	925	2.5
<sup>14</sup> N	2.0	1137	3.6
<sup>13</sup> C	3.0	951	5.4
<sup>12</sup> C	3.8	912	6.2
<sup>11</sup> C	4.6	878	7.0
<sup>10</sup> B	5.4	643	9.9
<sup>8</sup> Be	6.4	400	15.7
<sup>6</sup> Li	6.8	215	26.7
<sup>4</sup> He	6.0	77	48.5
<sup>3</sup> He	4.7	89	38.8
<sup>2</sup> H	2.5	14	68.9

Cancers 2015,7 Tommasino & Durante

# The FOOT Experimental setup

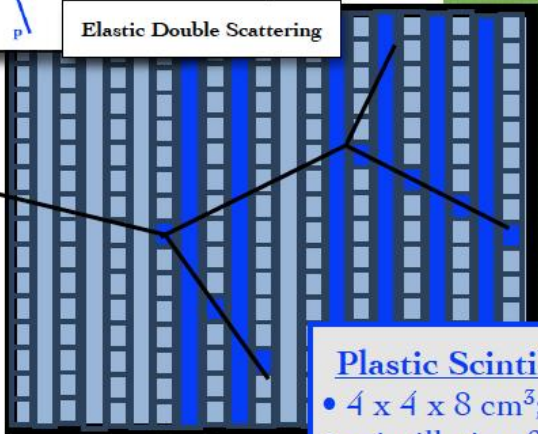
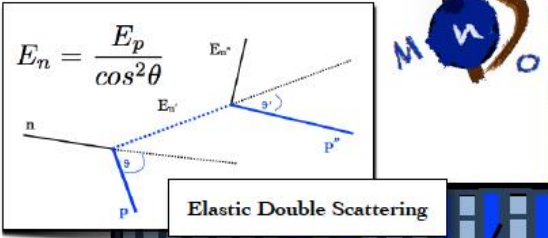


Expected performances:

- Resolution on fragment X-section < 5%
- Energy resolution < 1 MeV/u
- Measurements of Z with mistag < 3%
- Measurement of A with mistag < 5%

# MONDO (Fast Neutron Detection)

## High energy neutron detector



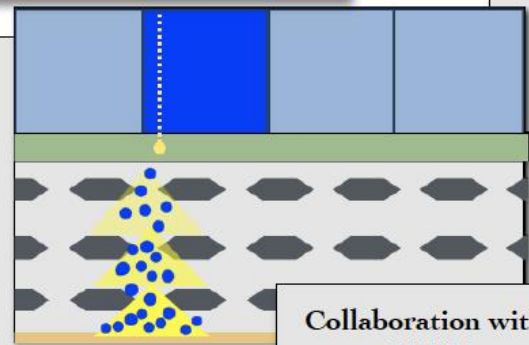
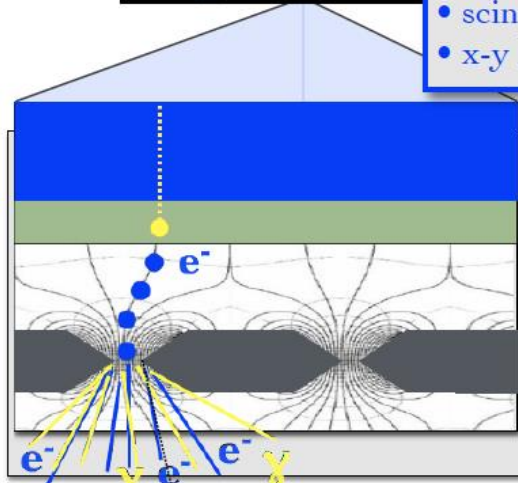
- Plastic Scintillator**
- 4 x 4 x 8 cm<sup>3</sup>;
  - scintillating fibres 250 μm;
  - x-y layer orientation;

In a particle therapy treatment the beam interactions with patient produce many secondary particles. Monitoring methods using photons and charged particles have already been proposed, but no attempt has been made yet to use the abundant neutron component. The large penetrating power of neutrons produces nearly energy threshold free escape, providing a secondary particle sample that is higher in number with respect to photons and charged particles. Therefore, neutrons allow for a backtracking of the emission point that is not affected by multiple scattering.

Moreover The neutron induced complications are the main concerns in Particle Therapy administration and planning, in particular in pediatric treatments [1].

We want to measure and track the ultra-fast neutrons produced in Particle Therapy treatments developing a **tracking device** tailored for hadrontherapy dose monitoring applications!

[1] M.Durante W.D. Newhauser doi:10.1038/nrc3069

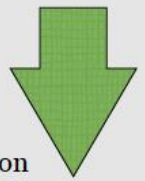


**Image Intensifier: Triple GEM detector**

**Gas Electron Multiplier**

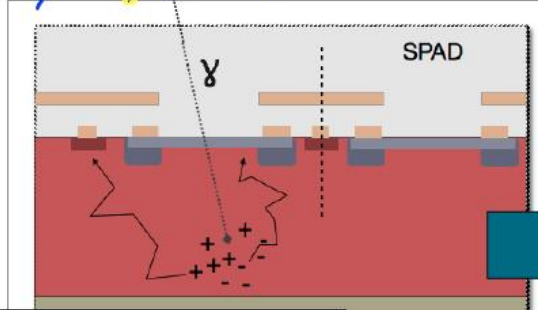
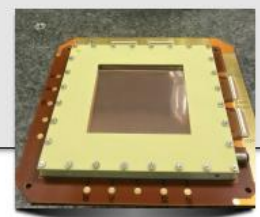
- 45 μm hole
- 70 μm hole distance
- triple GEM

We use GEM as photon intensifier instead of look for electron multiplication



Collaboration with CERN

For GEM light measurements => See also D.Pinci POSTER



- ✓ integrated TDC (resolution ~65 ps)
- ✓ self triggered sensor
- ✓ pixel 600 μm

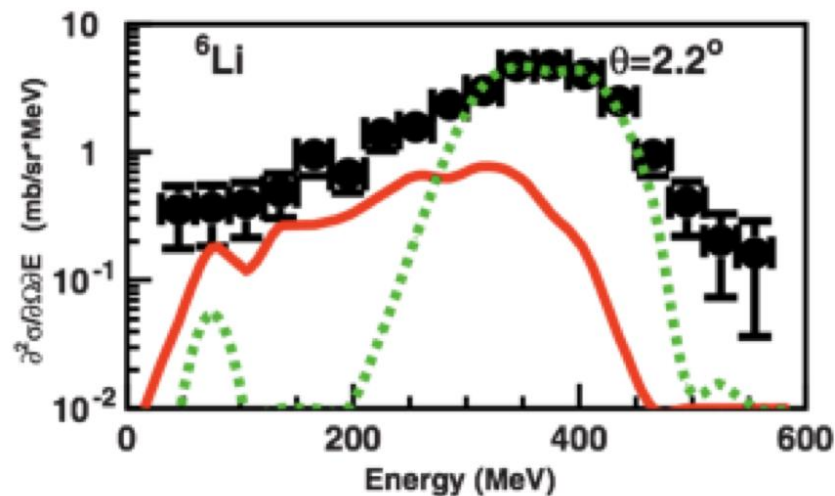
**Signals ReadOut: CMOS Single Photon Avalanche Diode (SPAD) array sensor**



- Despite the numerous and relevant application would use it, there is no dedicated model to nuclear interaction below 100 MeV/A in Geant4
- Many papers showed the difficulties of Geant4 in this energy domain:
  - Braunn et al. have shown discrepancies up to one order of magnitude in  $^{12}\text{C}$  fragmentation at 95 MeV/A on thick PMMA target
  - De Napoli et al. showed discrepancy specially on angular distribution of the secondaries emitted in the interaction of 62 MeV/A  $^{12}\text{C}$  on thin carbon target
  - Dudouet et al. found similar results with a 95 MeV/A  $^{12}\text{C}$  beam on H, C, O, Al and Ti targets

- **Exp. data**
- **G4-BIC**
- **G4-QMD**

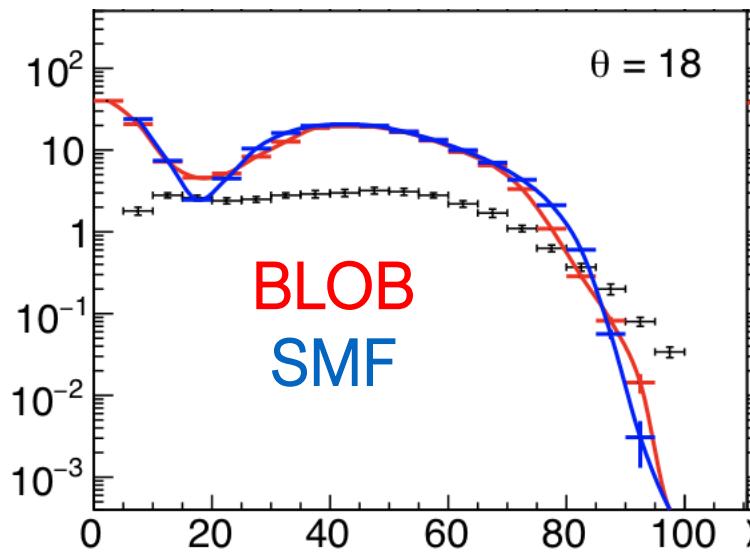
[Plot from De Napoli et al. Phys. Med. Biol., vol. 57, no. 22, pp. 7651–7671, Nov. 2012]



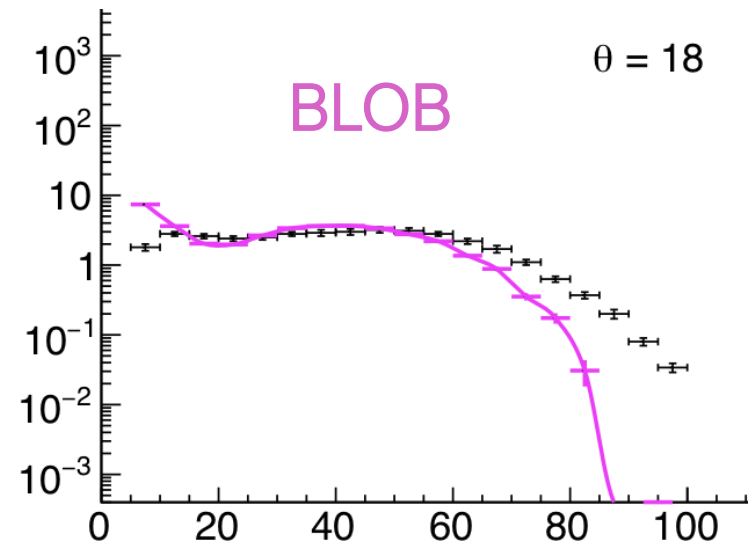
Cross section of the  $^6\text{Li}$  production at 2.2 degree in a  $^{12}\text{C}$  on  $^{nat}\text{C}$  reaction at 62 MeV/A.

# GENIALE: results

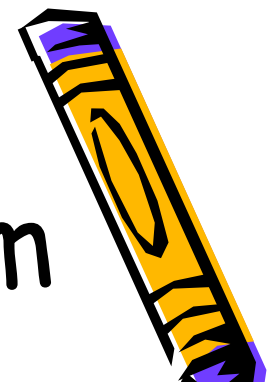
## Example: alpha production



- COALESCENCE
- EXITATION ENERGY CORRECTION

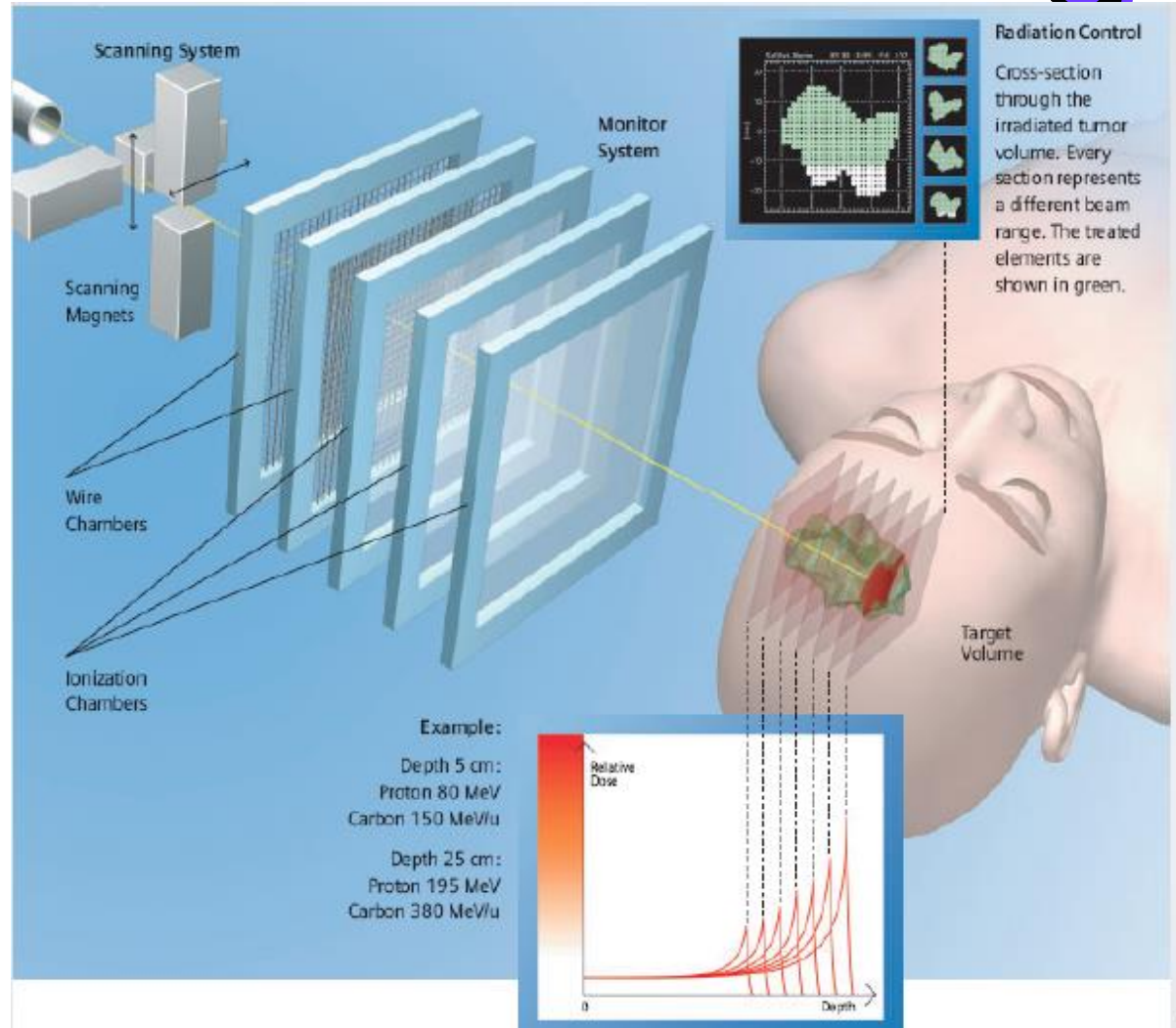






# Treatment Planning System

From the tumor margin to the beam sequencing ("Raster Scan")



# Use of GPUs

Typical times:

- Full MC 72hr
- Analytical commercial sw: 1hr
- GPUs → 1min



## Algorithm 3.2.2 Loop 1

```
1: for  $i = 0$  to  $N_{beams}$  do
2:   for  $j = 0$  to  $N_{beamlets}[i]$  do
3:      $currentBeamlet \leftarrow j + ptr$ 
4:     calculate and store angle  $\theta$ 
5:     calculate and store radiological depth  $d$ 
6:     compute and store input and output body points
7:   end for
8:    $ptr \leftarrow ptr + N_{beamlets}[i]$ 
9: end for
```

## Algorithm 3.2.1 Original Dose Calculation

```
1: for  $i = 0$  to  $N_{beams}$  do
2:   for  $j = 0$  to  $N_{beamlets}[i]$  do
3:      $currentBeamlet \leftarrow j + ptr$ 
4:     calculate angle  $\theta$ 
5:     calculate radiological depth  $d$ 
6:     compute input and output body points and corrections  $W_1, W_2$ 
7:     for  $ivoxel = 0$  to  $N_{voxels}$  do
8:       calculate parameters to dose calculation
9:       compute  $F_x$ 
10:      calculate dose  $D(\vec{r})$ 
11:     end for
12:   end for
13:    $ptr \leftarrow ptr + N_{beamlets}[i]$ 
14: end for
```

Split algo to  
parallelize

## Algorithm 3.2.4 Kernel Loop

```
1:  $threadIdx, blockIdx$ 
2: for  $i = 0$  to  $N_{beams}$  do
3:   for  $j = 0$  to  $N_{beamlets}[i]$  do
4:     calculate  $x$  and  $y$ 
5:     calculate parameters to dose calculation
6:     compute  $F_x$ 
7:     each thread calculates its dose contribution  $D(\vec{r})$ 
8:   end for
9:    $ptr \leftarrow ptr + N_{beamlets}[i]$ 
10: end for
```

# Hardware and Performance

		Threads	primary/s	$\mu\text{s}/\text{primary}$
CPU <sup>a</sup>	<b>full-MC</b> *	1	0.75 k	1340
	FRED	1	15 k	68
	FRED	16	50 k	20
	FRED	32	80 k	12.5
GPU	FRED	1 GPU <sup>1</sup>	500 k	2
	FRED	2 GPU <sup>2</sup>	2000 k	0.5
	FRED	4 GPU <sup>3</sup>	20000 k	0.05

Table A1: Computing times for different hardware architectures.

<sup>a</sup> motherboard with two Intel<sup>®</sup> Xeon E5-2687 8-Core CPU at 3,1GHz

<sup>1</sup> LAPTOP: Apple<sup>®</sup> MacBook Pro with one AMD<sup>®</sup> Radeon R9 M370X.

<sup>2</sup> DESKTOP: Apple<sup>®</sup> Mac Pro with two AMD<sup>®</sup> FirePro D300.

<sup>3</sup> WORKSTATION: Linux box with four NVIDIA<sup>®</sup> GTX 980.

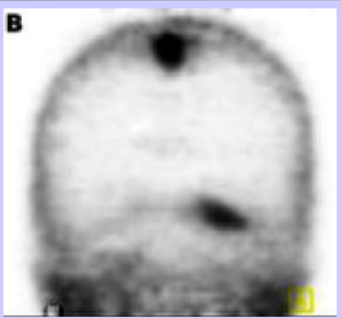
# NUCLEAR MEDICINE



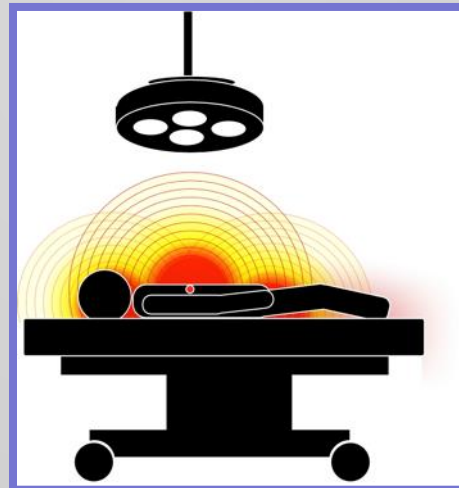
# Radio Guided Surgery

PET/SPECT scan to estimate receptivity and background

Each tumor requires its own tracer



Administration of radio-tracer



During surgery a probe is used to detect residuals/lymph nodes



Probe adjustable to needs



# LIMITS OF $\gamma$ -RGS

140 keV photons  
→ attenuation in body ~8cm

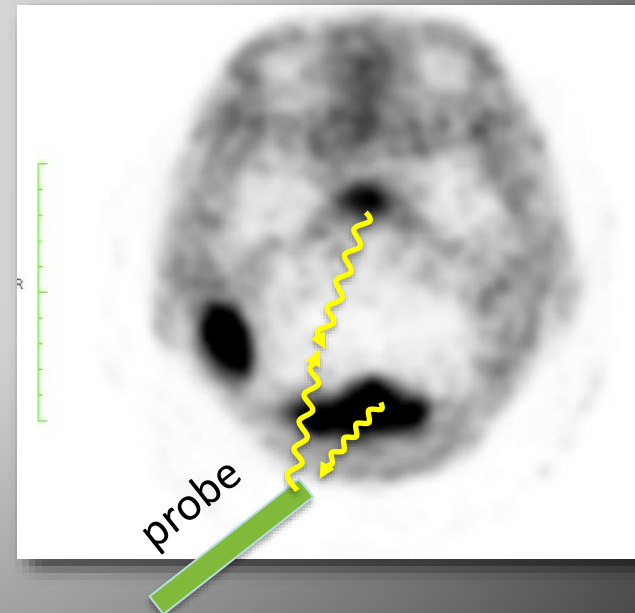
Long range of gamma's involve:

- exposure of medical personnel
- Background from healthy organs



Difficult to apply in:

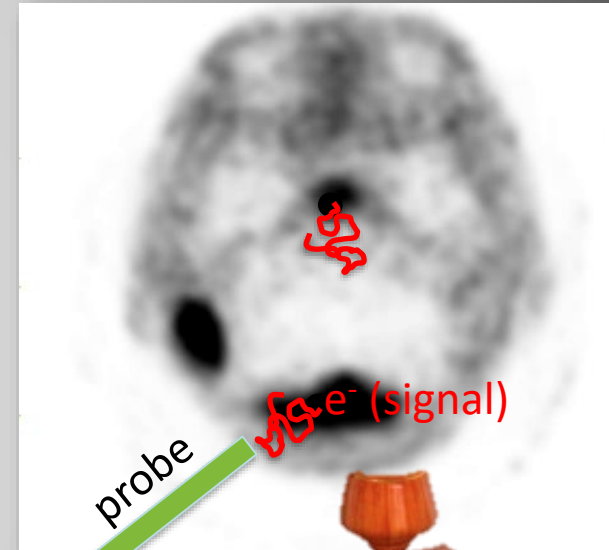
- Brain tumors
- Abdominal tumors
- Pediatric tumors



# A CHANGE IN PARADIGM

- Use of  $\beta^-$  tracers (electrons): pros
  - Detect electrons that travel  $\sim 100$  times less than  $\gamma$
  - Tracers with  $^{90}\text{Y}$  can be used (already used for Molecular RT)
  - No background from gamma
    - Shorter time to have a response
      - » Smaller administered activity
    - Smaller and more versatile detector
    - reduced effect of nearby healthy tissues
    - Reduced dose to medical staff

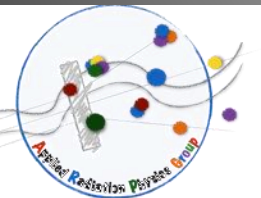
E. Solfaroli Camillocci et al, Sci. Repts. 4,4401 (2014)



NOTE: only detection at contact is possible



EXTEND RGS TO MORE CLINICAL CASES



# The probe prototype

Compact, easy to handle,  
local measurement

Simple technology:

- scintillating crystal
- Light sensor (SiPM)

Most stringent constraints:

- Mechanics
- electrical safety
- sterilization

Ongoing R&D:

- Detector improvements to lower energy threshold
- Laparoscopic application (adjustment in size, multiple reading for information from the side)

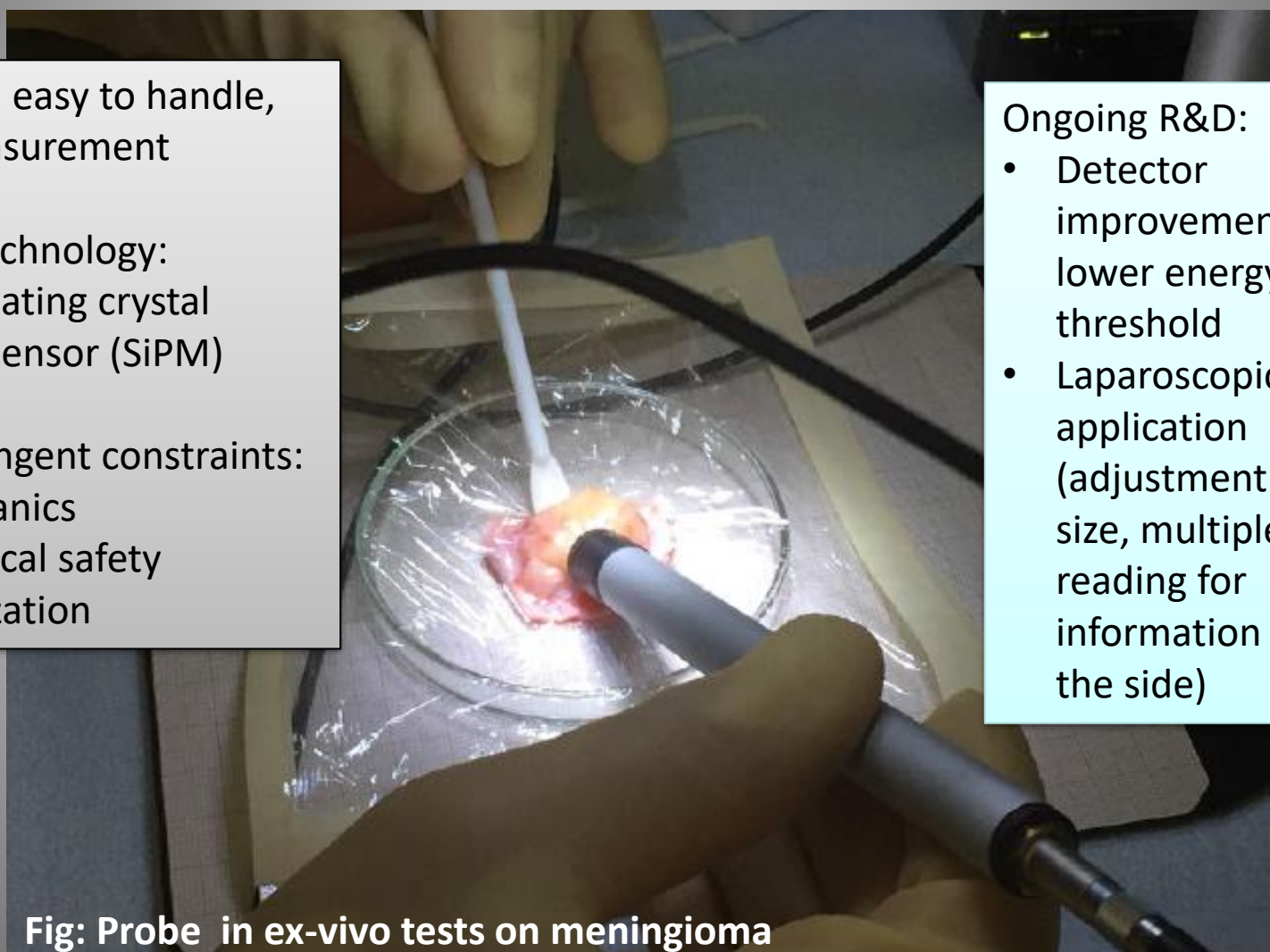
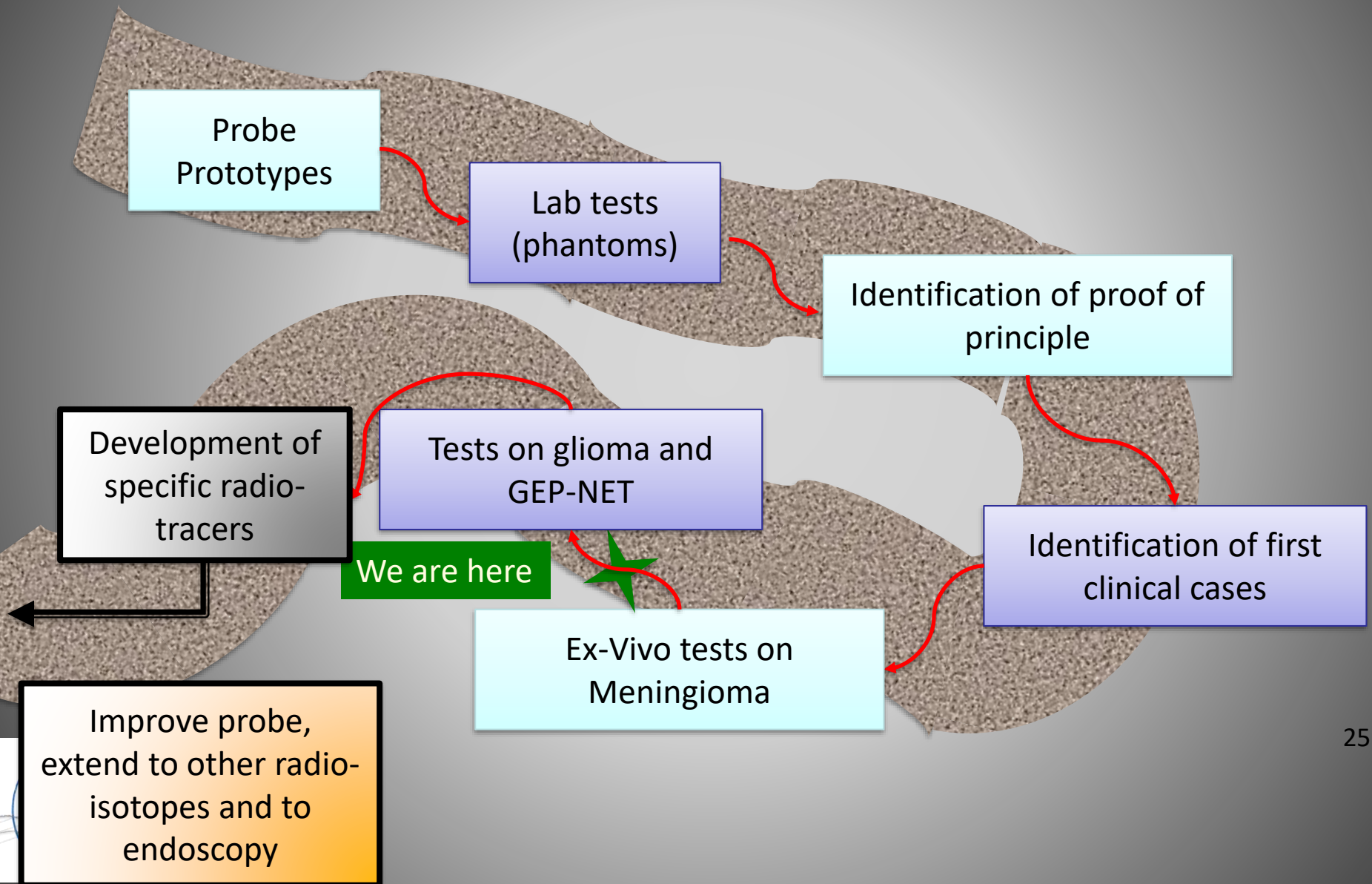


Fig: Probe in ex-vivo tests on meningioma





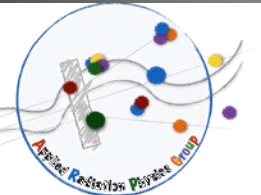
# RESEARCH PATH



# Perspectives

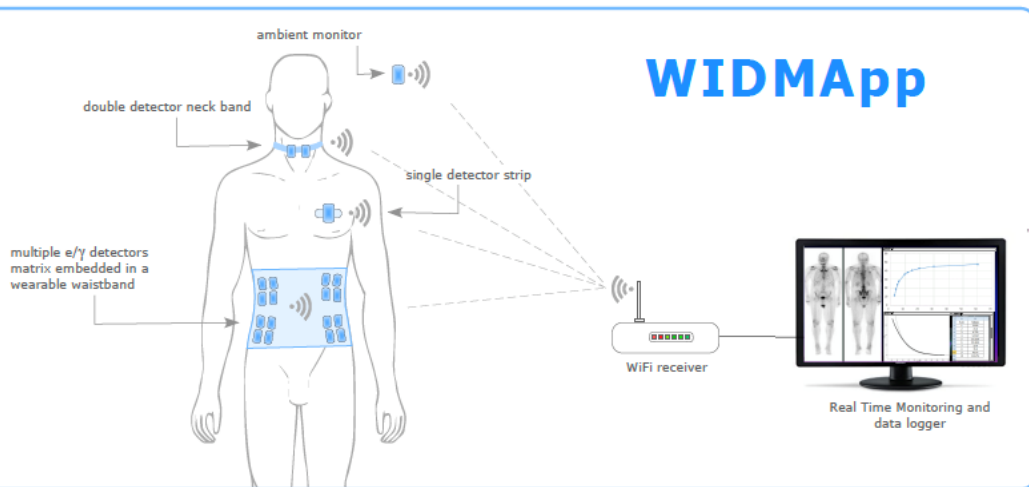
## Application to other radio-tracers

- $^{68}\text{Ga}$  in prostate cancer
- Development of a CMOS sensor based device
  - Extend to more radionuclides → more tumors



# Dosimetry in Target Radio Therapy

- TRT: Injection of radio-tracer that links preferentially with tumor → beta- radiation for therapy
- Need to certify acquired dose on patient-by-patient basis



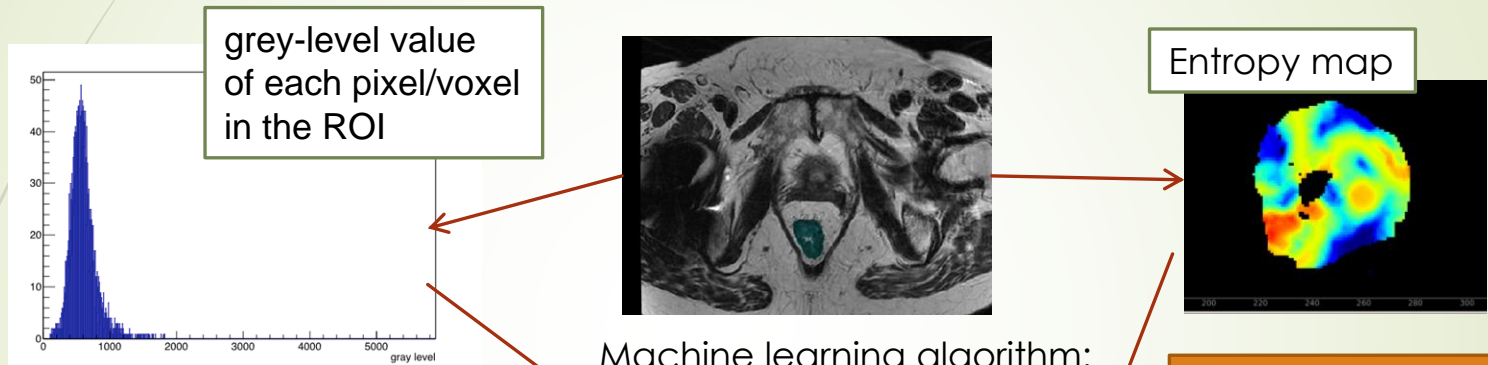
Development of sensors  
(evolution of the probe)

MC simulation/data analysis  
→ proof of principle

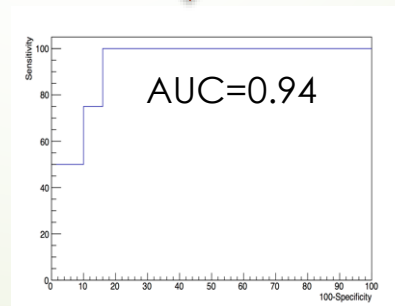
# ARTIFICIAL INTELLIGENCE IN MEDICINE



# Automatic classification of response to chemoradiotherapy in rectal cancer using 3T T2-w MRI



Avoid surgery to 50% of patients that would not need it



S. Ciardiello, RF, R. Paramatti, C. Mancini Terracciano, C. Voena, et al ...

Paper to be submitted to Radiology

Texture analysis of MR images

# Tomotherapy Quality assurance

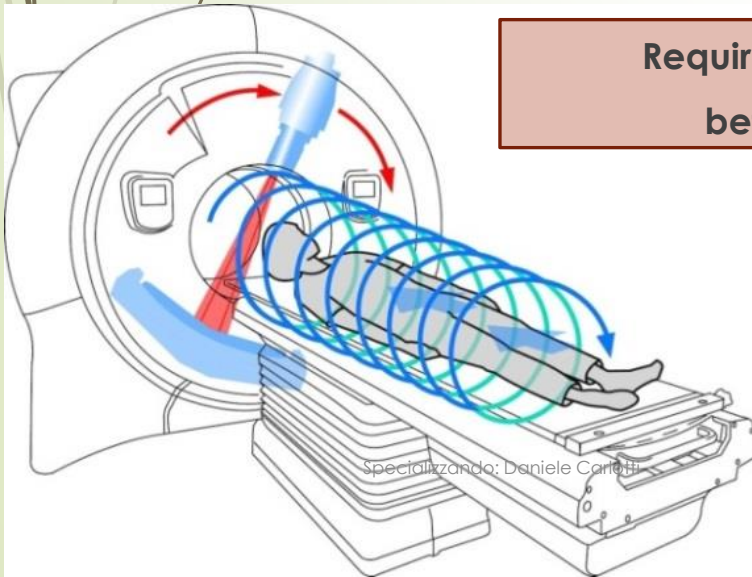
Tomotherapy (radiotherapy by slices) is a radiotherapy with very accurate dose profiling



Complex dose delivery



Requires accurate verification of correspondence between estimated and measured activity



# Application of Machine Learning

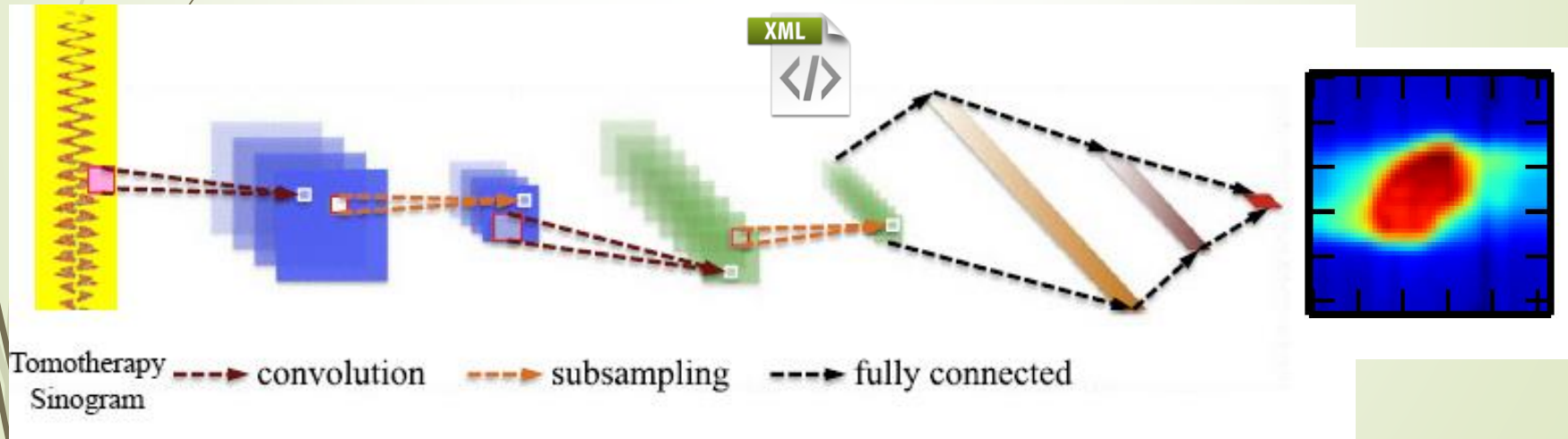
Aim of the study: develop an algorithm capable to estimate, patient by patient, the dose profile of TomoTherapy HiArt Delivery Quality Assurance (DQA)



Towards artificial QA

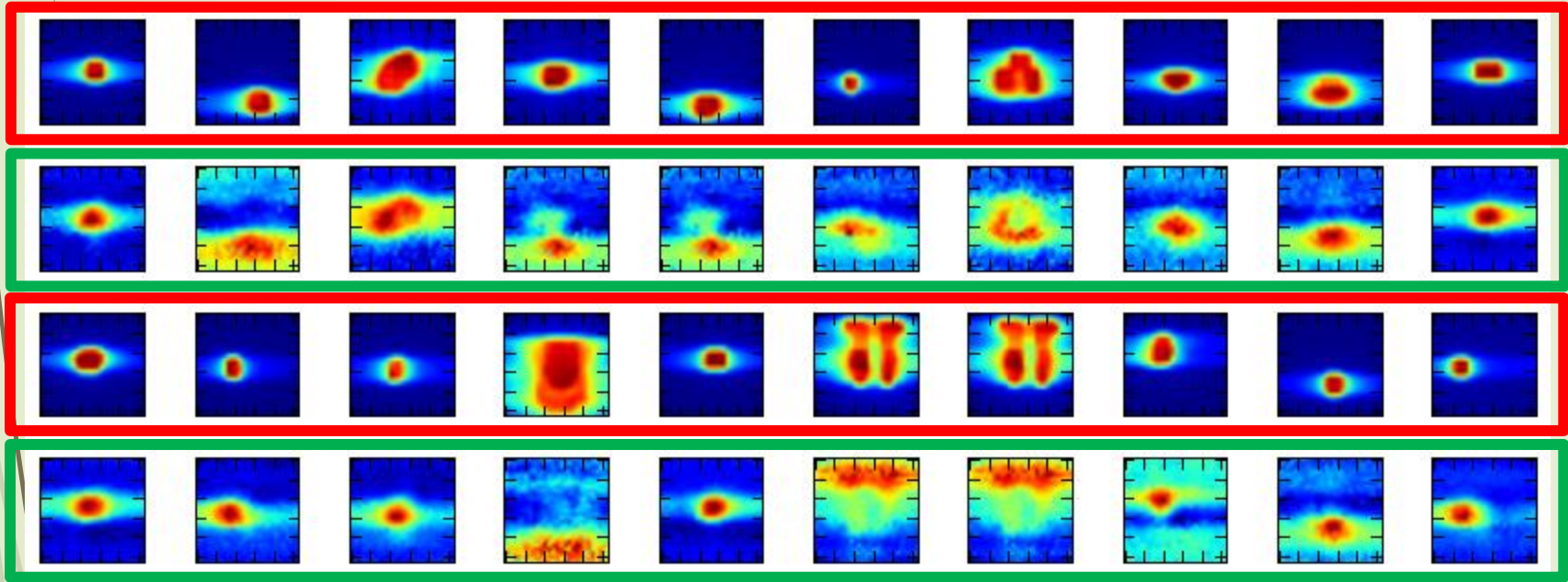
Raw Data

Dose profile



USE OF NNETS

# Virtual dose distribution

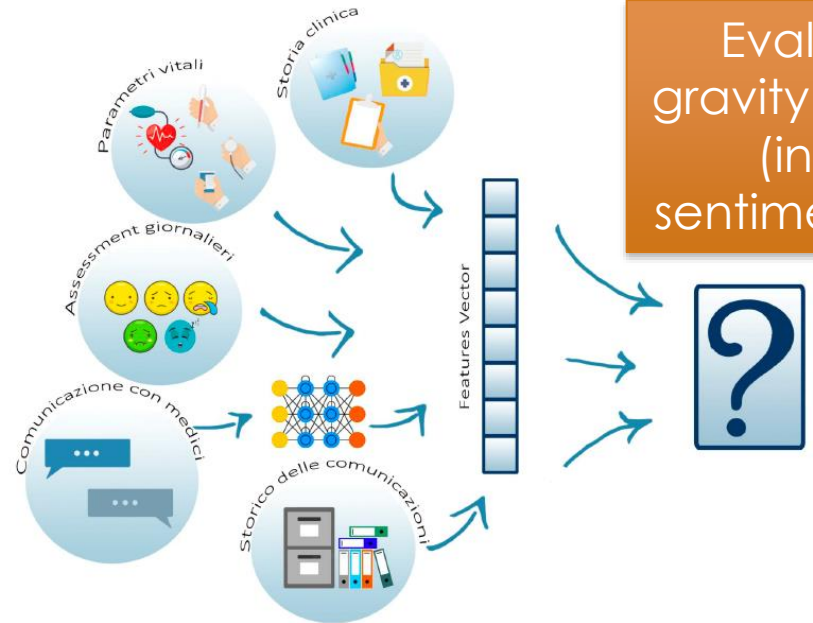


- In **red** measured images (sample of 729)
- In **green** images simulated with the developed neural network.



# Machine learning for patient–doctor interactions

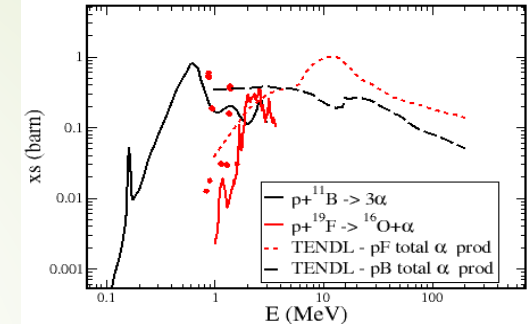
FILOBLU is an App to deal with post-operation follow-up @ home



- Machine Learning is required to
  - Automatic text analysis
  - Data Augmentation
  - Response classification



<b>Titolo</b>	<b>Nuclear process-driven Enhancement of Proton Therapy UNravEled</b>
<b>Area di ricerca</b>	<b>multidisciplinare</b>
<b>Responsabile nazionale</b>	<b>G Cuttone (INFN-LNS)</b>
<b>Unità partecipanti</b>	<b>LNS, Napoli, Roma1, Roma3, LNL, Milano, Pavia, TIFPA</b>



## PROJECT GOAL

Evaluate impact of <sup>19</sup>F and <sup>11</sup>B on particle therapy

## GOALS OF WP2 (IMAGING)

RM1

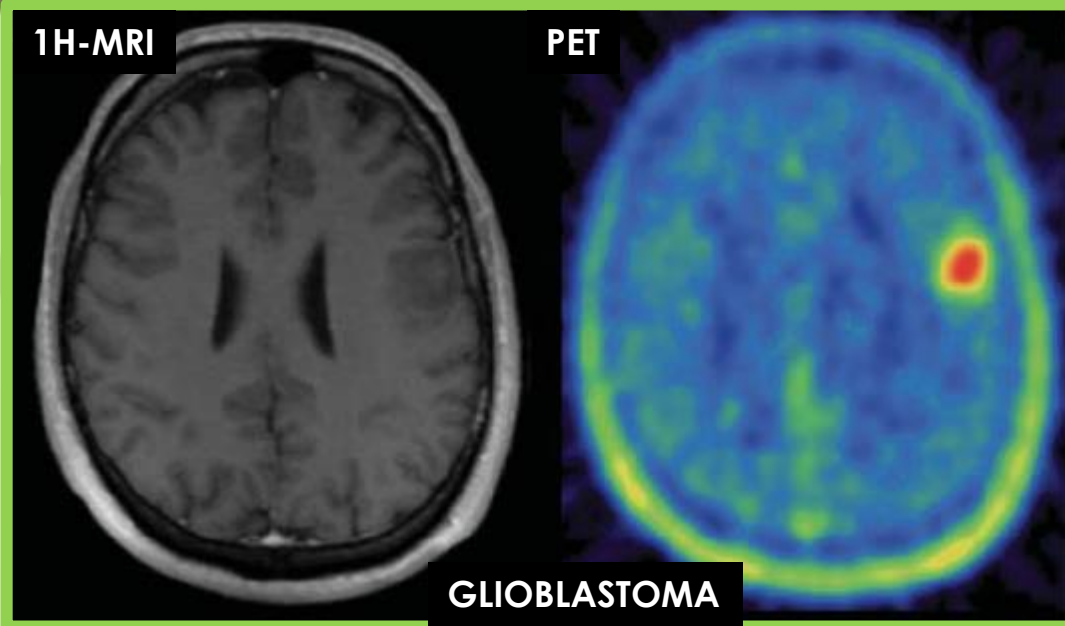
Evaluate bio-distribution of tracers

Evaluate concentration of samples

NA,P  
V

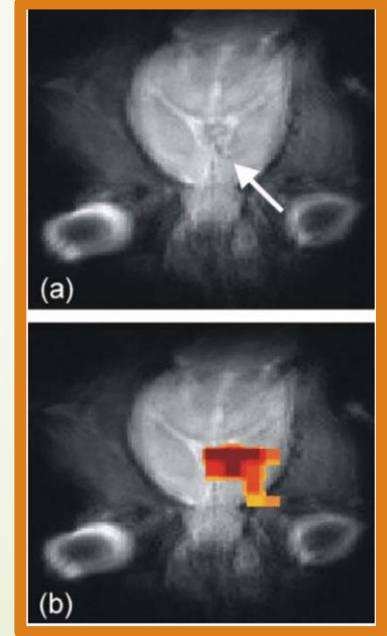
# Available techniques: PET/MRI

PET has a worse resolution and tracers more difficult to synthesize/handle but  $^1\text{H}$ -MRI does not show a signal ...



... but:

- gyromagnetic factor of  $^{19}\text{F}$  is only 6% away from  $^1\text{H}$
- $^{19}\text{F}$  is not present in human body (no physical background)



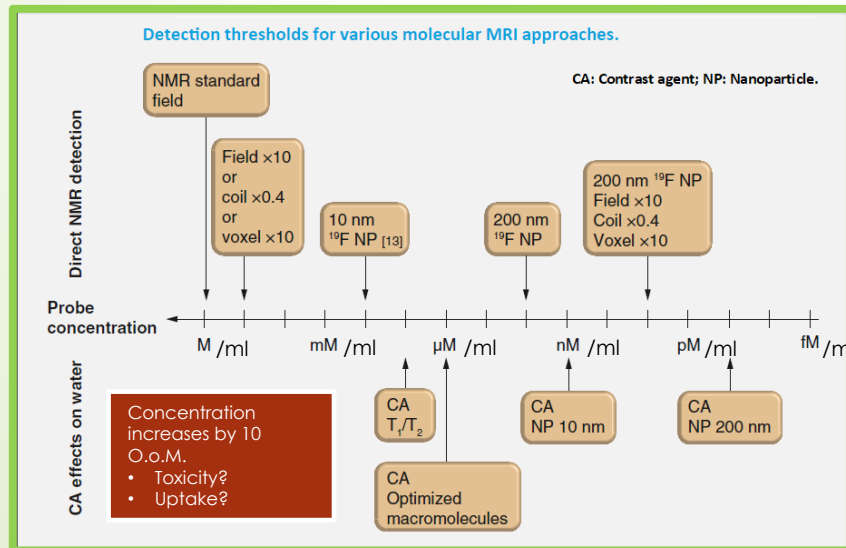
# Concentrations and Performances

## PET

- Typical PET activity concentrations:
  - Inject  $\sim 200\text{MBq}$  FDG (i.e.  $3 \cdot 10^{-12}$  moles), detect  $\sim 10^{-16}$  moles/ml

Cell Lines: PANCREAS(PANC-1)  
Tracers: BSH  
phenylalanine

## MRI



Concentrations required by Particle Therapy:

- 80 ppm
- 0.11 mg/ml
- 10  $\mu\text{M}/\text{ml}$

# Evaluation of bio-distributions of tracers

## THIS PROJECT

- A) Tests on animals to have samples with the correct concentration
- B) Setup a test stand to study and improve, with INFN competences, the signal/noise ratio



- C) Study co-registered  $^{19}\text{F}$  and  $^1\text{H}$  images to study the noise correlation and possible algorithms to enhance sensitivity to signal



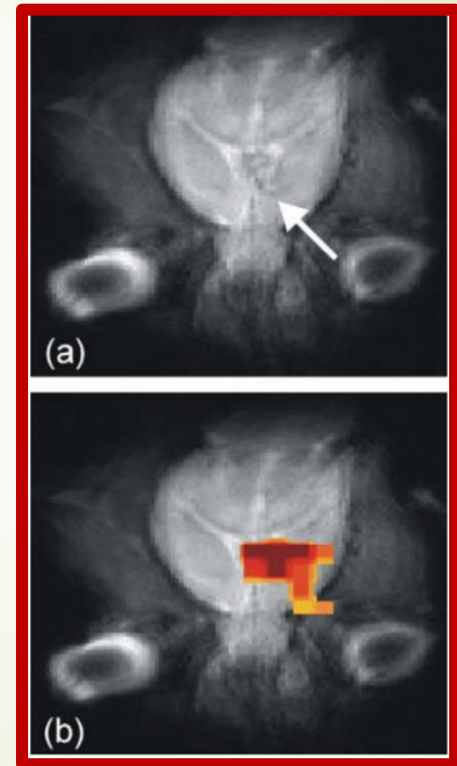
# Study of co-registered 1H-19F analyses

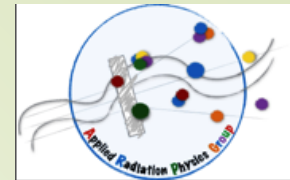
Currently 1H and 19F images are only superimposed for visual comparison (combination is just product of signals)



**Artificial Intelligence** needed to:

- Align images
- Use autoencoders as de-noisers
- Segment 1H images
- Data augmentation





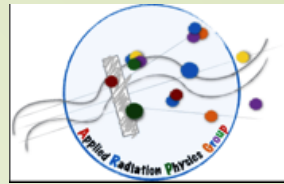
# Possibili tesi di laurea

## HARDWARE:

- Sviluppo e test di rivelatori
  - Assemblaggio
  - Machining componenti (stampante 3D)
- Setup e acquisizione dati di test NMR
- Setup e acquisizione dati test clinici o pre-clinici

## SOFTWARE:

- Analisi dati esperimenti su fascio, fantoccio, animali pazienti
- Applicazioni Machine Learning
- Simulazioni Monte Carlo
- Sviluppo di software
  - per simulazioni
  - Per ricostruzione esperimenti



## Possibili tesi di laurea

NUCL MED

- Studio di fattibilità della matrice di sensori (WIDMApp): simulazioni MC, analisi dati e test su fantoccio
- Analisi test clinici e pre-clinici sonda intraoperatoria (CHIRONE) Contatto: elena.solfaroli@roma1.infn.it, francesco.collamati@roma1.infn.it

HADRON TH

- Caratterizzazione di nuovi scintillatori plastici per lo sviluppo di fast timing detector e/o pulse shape discrimination.
- Test del sensore e ricostruzione degli eventi di MONDO
- Sviluppo della camera a coppie (PAPRICA)
- Studio performance dei rivelatori di FOOT su TestBeam
- implementazione in FRED dei modelli di interazione di elettroni e fotoni per la IORT. Contatto: alessio.sarti@roma1.infn.it, vincenzo.patera@roma1.infn.it

ART INTEL

- Studio del segnale analogico delle antenne NMR tramite Software Designed Radio (NEPTUNE)
- Applicazione del machine learning alle immagini NMR con 19F (NEPTUNE)
- Applicazione del machine learning alla stadiazione dei tumori (MARIANNE) Contatto: cecilia.voena@roma1.infn.it, stefano.giagu@roma1.infn.it